



## Original Article

# Development Characterization and Evaluation of Nasal *in situ* Gel containing Anti-Asthmatic Drug

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### ARTICLE INFO

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**Objective:** The purpose of the present study is to develop, characterize and evaluate nasal *in situ* gel containing anti-asthmatic drug of Cromolyn Sodium

**Method:** Ion activated method was used for the preparation of *in situ* gel, and gellan gum is used as ion triggered polymer. *In-situ* gels Cromolyn Sodium with Gellan Gum as a gelling agent, PVP K30, HPMC K 100 M and Lutrol F127 as polymer. The formulations were evaluated for gel formation, pH, viscosity, *in vitro* release, drug content, and mucoadhesive force.

**Results and Discussion:** pH of all the formulations were found to be in the range of 6.0 - 6.55 and the drug content for all the prepared formulations were found to be in the field of 80 - 92%. The results of *in vitro* drug release indicated that the optimized formulation F6 is the utmost successful formulation of the study, revealed a sustained drug release of 92% in 24 hours.

**Conclusion:** It can be settled that Cromolyn Sodium nasal *in situ* gel produces prolonged and site-specific drug delivery for the treatment of Asthma.

**Keywords:** Ion activated method, Cromolyn Sodium, Gellan Gum, Lutrol F-127, HPMC K100 M, and PVP K 30.

## 1. INTRODUCTION

Nasal gels are high-viscosity thickened solutions or suspensions. The advantages of a nasal gel include the reduction of post-nasal drip due to high viscosity, reduction of taste effect due to reduced swallowing, reduction of anterior leakage of the formulation, modification of irritation by using soothing/emollient excipients and target to mucosa for better absorption. In-Situ gelation is a process of gel formation at the site of action after the formulation has been applied at the site. In-Situ gel phenomenon based upon liquid solution of drug formulation and converted into the semi-solid mucoadhesive key depot. It permits the drug must be delivered in a liquid form or solution form.

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In situ gel formation of drug delivery systems can be defined as a liquid Formulation generating a solid or semisolid depot after administration. In situ activated gel-forming Systems are those which are when exposed to physiological conditions will shift to a gel phase. Gelation occurs via the cross-linking of polymer chains that can be achieved by covalent bond formation (chemical cross-linking) or Non-covalent bond formation (physical cross-linking). The impact of external stimuli such as temperature, pH, and ionic strength, on the cross-linking of polymer chains have been studied to improve the gel strength or to induce in situ gelations. Both natural and synthetic polymers can be used for the production of *in situ* gels

**Principle of In-Situ Gel:** In situ gel-forming drug delivery systems is the principle, capable of releasing the drug in a Sustained manner maintaining relatively constant plasma profiles. Formulation of in-situ gel systems involves the use of a gelling agent which can form a stable sol/suspension system to contain the dispersed drug and other excipients. The gelling of this sol/suspension is to be achieved in the gastric environment, triggered by ionic complexation due to change in pH.<sup>1</sup>

**Importance of In-Situ Gelling System:**

- A low dose is required for treatment
- Minimum local and systemic side effects
- Ease of application
- Reduced frequency of drug administration
- Improved patient compliance and comfort
- Increased residence time
- Improved bioavailability<sup>2</sup>

Cromolyn Sodium acts by inhibiting the release of chemical mediators from sensitized mast cells. It is used in the prophylactic treatment of both allergic and exercise-induced asthma but does not affect an established asthmatic attack. The aim of the present study is to develop, characterize and evaluate of nasal in situ gel containing anti-asthmatic drug of Cromolyn Sodium

## 2. MATERIALS AND METHODS

**Materials:** Cromolyn Sodium from Swapnaroop Drugs &Pharmaceuticals, Mumbai. Lutrol F-127, HPMC K100M and PVP K 30 was from Hi-Media Laboratories Pvt. Ltd. Gellan Gum, Mannitol and Benzalkonium chloride was from SD Fine Chem Laboratories Pvt.

**Methodology**

**Standard Curve of Cromolyn Sodium with Nasal Simulated Fluid**

Cromolyn Sodium is a white powder which is soluble in water. Though several methods are reported for its estimation, the UV spectrophotometric method was employed in the study.

Cromolyn Sodium shows maximum absorbance at 326.6nm in simulated nasal fluid pH of 4.5. Based on this information, a standard graph was constructed (Figure No.1).

**Standard Curve of Cromolyn Sodium with Phosphate buffer**

Cromolyn Sodium shows maximum absorbance at 327nm in Phosphate buffer pH of 7.4. Based on this information, a standard graph was constructed (Figure No.2).

**FTIR STUDIES**

Infrared spectra of all the ingredients used in the formulation are taken individually. Also, the infrared spectrum of the physical mixture (*in situ* gel) is made. The application of infrared spectroscopy lies more in the qualitative identification of substances either in pure form or in the combinations and as a tool in the establishment of the structure. Since IR is related to covalent bonds, the spectra can provide detailed information about the structure of molecular compounds. In order to establish this point, comparisons are made between the range of the substance and the pure compound. The above discussions imply that infrared data is helpful to confirm the identity of the drug and to detect the interaction of the drug with the excipients. The samples are scanned between wavenumber ranges of 4,000 to 500 cm<sup>-1</sup>.

**Preparation of nasal *in-situ* gel Formulations by Ion Induced method**

Gellan gum (0.3%) solutions were prepared by adding the gum to deionized water and heating up to 70<sup>0</sup>C while stirring. After cooling to below 40<sup>0</sup>C, HPMC K 4 M, Cromolyn Sodium (1%,w/v), mannitol (4%, w/v), and Benzalkonium chloride (0.01%, w/v) are added and mixed well.<sup>3</sup>

**Evaluation of *in situ* gelling solution**

**Determination of pH**

The pH of gels is checked by using a digital pH meter at room temperature. Initially, the pH meter is calibrated using standard buffers of pH 4 and 7.0. 1ml of the gelling solution is taken vial (container), and then the made up to 10 ml with distilled water, the electrode of pH meter was dipped in the dispersion, and the pH is noted.

**Viscosity Measurement of the nasal *In Situ* Gelling Solution**

The viscosity was measured at 30±2<sup>0</sup>C using Brookfield viscometer (model name, RV DV2T) and spindle number T5 at 5-25 rpm. First, 50 ml of the in-situ gel was taken in 50 ml beaker, and the viscosity of the gel solution was measured. The reading obtained was noted.

**Evaluation of Cromolyn Sodium nasal *in situ* gels**

**Clarity**

The clarity of various formulations was determined by visual inspection under the black and white background, and it was graded as follows: turbid, +; clear, ++; and very clear (glassy), +++.

**pH of Formulation**

The pH of each formulation was determined by using pH meter (Equiptronics, Model EQ-610). The pH meter was first calibrated using solutions of pH 4.5 and 7.<sup>4</sup>

**Determination of Drug Content**

Uniform distribution of active ingredient is essential to achieve dose uniformity. The drug content is determined by taking 1 ml of the formulation to 100 ml volumetric flask. Then makeup with simulated nasal fluid up to the mark and shaken vigorously. From the above solution, 10 ml is withdrawn and further diluted to 100 ml with simulated nasal fluid. The absorbance of the above solution is measured at 326.6nm by using UV-Vis spectrophotometer.<sup>5</sup>

**Determination of Mucoadhesive Force**

The mucoadhesive strength of each formulation was determined by measuring the force required to detach the formulation from goat nasal mucosal tissue by using a modified chemical balance. A section of the nasal mucosa was cut from the goat's nasal cavity, and the mucosal side was instantly fixed into each glass vial using a rubber band. The vials with nasal mucosa were stored at 37°C for 5 minutes. Then next vial with a section of mucosa was connected to the balance in an inverted position while the first vial was placed on a height-adjustable pan. A fixed amount of sample of each formulation was placed onto the nasal mucosa of the first vial. Then the height of the second vial was adjusted so that mucosal surfaces of both vials come in intimate contact. Two minutes contact time was given to ensure close contact between tissues and the sample. Then weight was increased in the pan until vials got detached. The bioadhesive force, expressed as the detachment stress in dyne/cm<sup>2</sup>, was determined from the minimal weights that separated the tissues from the surface for each formulation using the following equation.

$$\text{Detachment stress (dyne/cm}^2\text{)} = m \times g / A$$

Where, m =Weight required for detachment of two vials in gm

g = Acceleration due to gravity [980cm/s<sup>2</sup>]

A = Area of tissue exposed

The nasal mucosa was changed for each measurement.<sup>5</sup>

**In vitro drug diffusion Studies**

*In-vitro* drug release study of in situ gel formulation is carried out by Franz diffusion cell of 22ml capacity. The formulation is 2 ml placed in the donor compartment and 22ml of freshly prepared simulated nasal fluid of pH 4.5 is placed in the receptor compartment. Between receptor and donor compartment, dialysis membrane previously soaked overnight in the diffusion medium is placed. The whole assembly is placed on a thermostatically controlled magnetic stirrer. The temperature of the medium at 37±0.5°C.2ml sample is withdrawn at a predetermined time interval of 1 hour for 24hrs. The sample volume of fresh medium is placed. The withdrawn samples are suitably diluted and by UV spectrophotometer at326.60nm using the simulated nasal fluid as blank.<sup>5</sup>

**Table 1: Formulation of Cromolyn Sodium nasal *in situ* gel (F1-F9)**

INGREDIENT	F1	F2	F3	F4	F5	F6	F7	F8	F9
<b>S</b>									
<b>Cromolyn Sodium(mg)</b>	100	100	100	100	100	100	100	100	100
<b>Gellan Gum(mg)</b>	30	30	30	30	30	30	30	30	30
<b>HPMC K 100</b>	2	5	10	-	-	-	-	-	-
<b>M(mg)</b>									
<b>PVP K30(MG)</b>	-	-	-	2	5	10	-	-	-
<b>Lutrol 127(mg)</b>	F-	-	-	-	-	-	2	5	10
<b>Mannitol(mg)</b>	400	400	400	400	400	400	400	400	400
<b>Benzalkonium chloride(ml)</b>	0.002 ml	0.002 ml	0.002ml	0.002 ml	0.002 ml	0.002ml	0.002 ml	0.002 ml	0.002ml
<b>Distilled water q.s to</b>	10ml	10ml	10ml	10ml	10ml	10ml	10ml	10ml	10ml

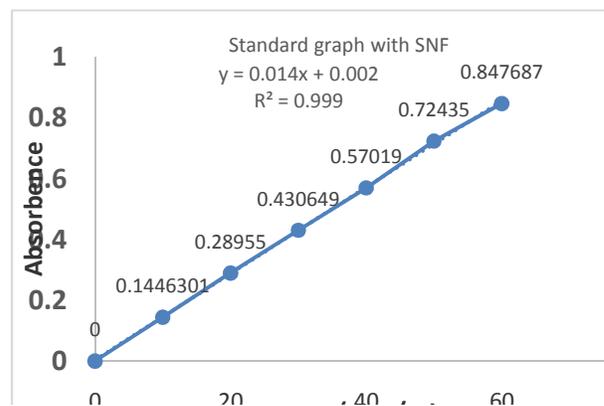
**3. RESULTS AND DISCUSSION**

**Calibration curve of Cromolyn Sodium in simulated nasal fluid**

The absorbance of standard solutions of Cromolyn Sodium at 326.6 nm to plot calibration curve in the simulated nasal fluid.

**Table 2: Data for the standard graph of Cromolyn Sodium at 326.6 nm in Nasal Simulated Fluid**

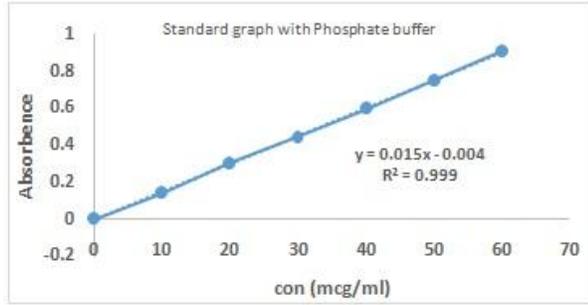
Concentration (µg/ml)	Absorbance at 326.6 nm
10	0.146301
20	0.285950
30	0.430649
40	0.570190
50	0.724350
60	0.84787



**Fig 1: Standard graph of Cromolyn Sodium at 326.6 nm in simulated nasal fluid**

**Calibration curve of Cromolyn Sodium in Phosphate buffer:**

The absorbance of standard solutions of Cromolyn Sodium at 327 nm to plot calibration curve in Phosphate buffer.



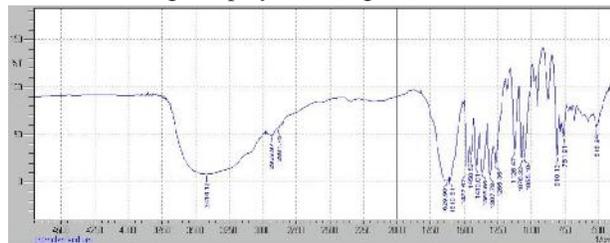
**Fig 2: Standard graph of Cromolyn Sodium at 327 nm in Phosphate buffer**

**Table 3: Data for the standard figure of Cromolyn Sodium at 327 nm in Phosphate buffer**

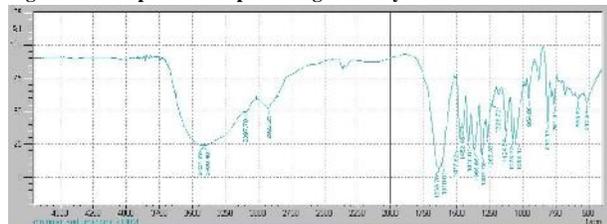
Concentration (mcg/ml)	Absorbance at 327nm
10	0.142883
20	0.302628
30	0.442078
40	0.597931
50	0.750717
60	0.910004

**FTIR STUDIES**

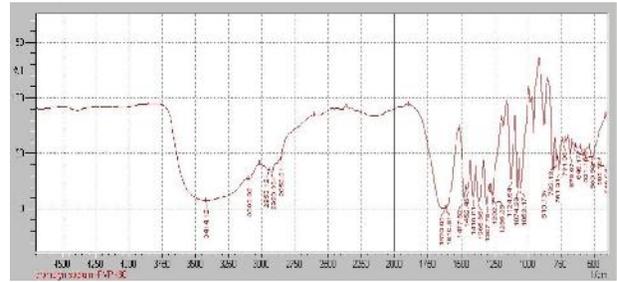
FT-IR spectra of pure Cromolyn Sodium, and combination with HPMC K100 M, PVP K30 were shown in the (Figure No.3-5). Pure Cromolyn Sodium showed principal absorption peaks at 3414.12 cm<sup>-1</sup> (-OH stretching), 2929.97cm<sup>-1</sup> (-CH Ali stretching), 1629.90 cm<sup>-1</sup> (>C=O stretching), 1477.00 cm<sup>-1</sup> (-CH<sub>2</sub> bending), and 1265.35 cm<sup>-1</sup> (-CH<sub>3</sub> bending). Same peaks of C=O, -OH, C-H, -CH<sub>2</sub> and -CH<sub>3</sub> bonds were present as that of the pure drug without much shifting in the spectra of Cromolyn Sodium along with the polymers. This suggested no chemical interaction between the drug and polymers. (Fig 3-5)



**Fig 3: FT-IR Spectrum of pure drug Cromolyn Sodium**

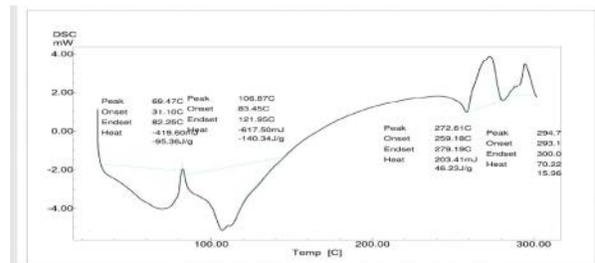


**Fig 4: FT-IR Spectrum of pure drug Cromolyn Sodium + HPMC K100 M**

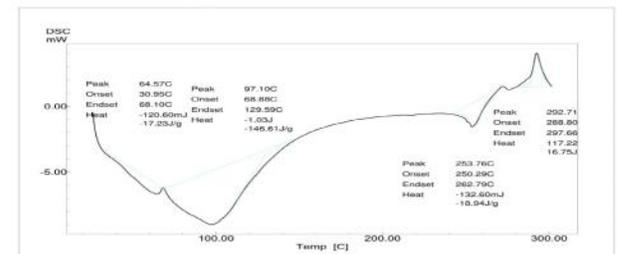


**Fig 5: FT-IR Spectrum of pure drug Cromolyn Sodium + PVP K30**

**DSC Studies**  
In order to find out drug and out excipients compatibility DSC studies were also accomplished. Pure Cromolyn Sodium exposed sharp endothermic peak at 272.61°C. The DSC studies curve of Drug and PVP K30 mixture demonstrated an endothermic peak at 253.76°C. But in the formulation, there was a slight change in peak temperature, which might be due to the mixing of the drug and excipients, which could have reduced the purity level of each component. But DSC results did not show any major interaction.



**Fig 6: DSC curve of pure drug Cromolyn Sodium**



**Fig 7: DSC curve of drug and PVP K30**

**Evaluation of Cromolyn Sodium nasal *in situ* gelling solution:**

**Table 4: Evaluation report of the gelling solution (F-1 to F-9).**

PARAMETERS	FORMULATION CODE								
	F1	F2	F3	F4	F5	F6	F7	F8	F9
Colour	Colour Less	Colour Less	Colour Less	Colour Less	Colour Less	Colour Less	Colour Less	Colour Less	Colour Less
pH	6.23	6.48	6.0	6.52	6.55	6.33	6.33	6.42	6.0
Viscosity in cps	96	185	443	81	166	431	103	196	480

The pH of the *in situ* gelling sol was found to be 6.0 to 6.55, and it was found to be acidic in nature. Viscosity was found to be in the range of 5 to 25 cps.

**Drug Content and Mucoadhesion:**

Drug content was estimated for all the batches, and it was found to be in the range of 80 – 92%. The results are shown in Table 5. It shows that as the concentration of HPMC K100M, PVP K30, and Lutrol F 127 increases, the bioadhesive strength also rises. The mechanism of bioadhesion can be attributed to hydrogen bonding between gel formulation and oligosaccharide chains of the mucosal membrane. The mucoadhesive force of prepared formulation is in the range of 1248.4 dyn/cm<sup>2</sup> to 2496.8 dyn/cm<sup>2</sup>.

**Table 5: Evaluation report of *in situ* gel (F-1 to F-9)**

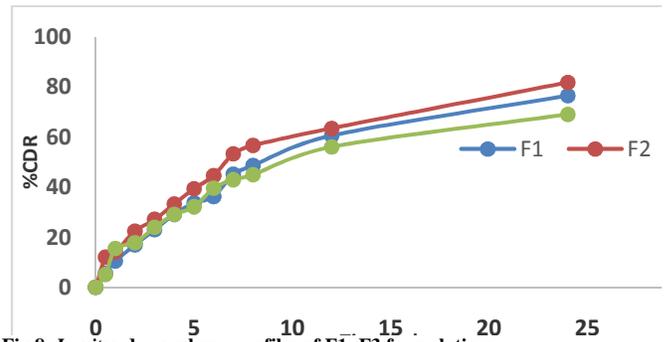
PARAMETER	F1	F2	F3	F4	F5	F6	F7	F8	F9
Clarity	+++	+++	+++	+++	+++	+++	+++	+++	+++
pH	6.23	6.48	6.0	6.52	6.55	6.33	6.33	6.42	6.0
Drug content (%)	85	89	82	84	84	92	80	82	81
Mucoadhesive force in dyn/cm <sup>2</sup>	1404.4	1560.5	1872.6	1248.4	1248.4	2496.8	1778.9	2184.7	1560.5

**In Vitro Release Study:**

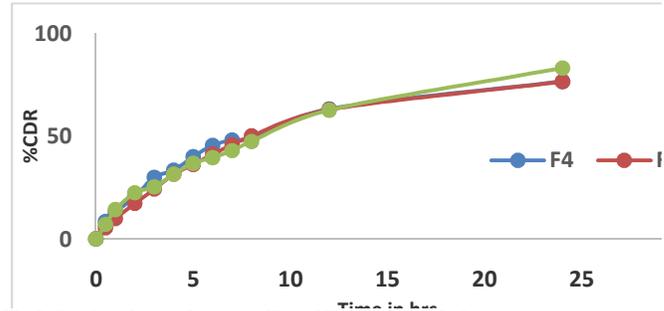
*In vitro* release studies were carried out for all the formulations using Franz diffusion cell with dialysis membrane engaging magnetic stirrer at 50rpm. It was conducted in SNF. The results were evaluated for 24 hours. The *in situ* gels of different formulations were evaluated for pH, viscosity, drug content, and *in vitro* release. The results of all the formulations for different tests found to be within limits. Upright uniformity in drug content was found among different batches of *in situ* gel. The release studies were carried out for all the formulations. The formulations were prepared by increasing the concentration of the mucoadhesive polymer. The formulation which shows the percentage of drug release maximum at 24 hrs was considered as optimum. The percentage drug release of all prepared formulation is in the range of 57.44 to 83.12, were presented in (Table 6) and (Fig 8-10).

**Table 6: Percentage Drug Release of Formulations F-1 to F-9**

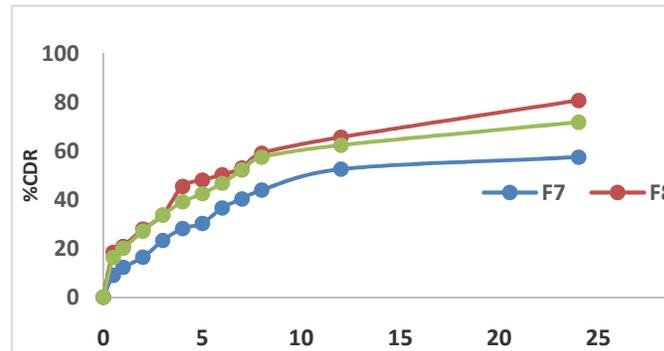
Time (hrs)	FORMULATIONS								
	F1	F2	F3	F4	F5	F6	F7	F8	F9
0	0	0	0	0	0	0	0	0	0
0.5	5.636	12.07	5.12	8.51	5.33	7.06	8.99	18.45	16.31
1	10.49	14.26	15.46	12.98	9.93	14.26	12.26	20.79	20.06
2	16.98	22.43	17.79	20.71	17.26	22.46	16.39	27.96	27.03
3	23.00	27.13	24.00	29.94	24.25	25.34	23.23	33.76	33.72
4	29.17	33.33	29.13	33.43	31.45	31.49	28.16	45.45	39.12
5	33.70	39.42	32.16	40.04	36.19	36.81	30.28	48.07	42.43
6	36.28	44.63	39.00	45.46	41.23	39.52	36.59	50.25	46.72
7	45.24	53.35	43.00	48.15	45.71	42.94	40.34	53.03	52.21
8	48.69	56.69	44.95	48.99	50.05	47.41	43.94	59.09	57.45
12	60.59	63.51	56.06	63.17	62.89	62.63	52.52	65.64	62.35
24	76.59	81.85	69.07	76.60	76.50	83.12	57.44	80.73	71.77



**Fig 8: In-vitro drug release profiles of F1- F3 formulations**



**Fig 9: In-vitro drug release profiles of F4- F6 formulations**



**Fig 10: In-vitro drug release profiles of F7- F9 formulations**

**4. CONCLUSION**

In this study sustained-release nasal *in situ* gels of Cromolyn Sodium was prepared by ion-induced mechanism, using Gellan Gum as a gelling agent and PVP K30, HPMC K 100 M and Lutrol F 127 as mucoadhesive polymer. The formulation F6 containing 30mg of Gellan Gum and 10mg of the PVP K 30 showed proper drug release over a period of 24 hours. Based on the FT-IR studies, there appears to be no probability of interaction between Cromolyn Sodium and polymers/ other excipients used in the formulation. The entire formulations disclosed adequate quality control properties like Viscosity, pH, drug content, mucoadhesive force, etc. and conformed within the specifications for tested parameters. Thus, formulation F6 was found to be the most encouraging formulation on the basis of adequate *in situ* gelling properties. The formulated Systems provided sustained release of the drug over a 24-hour period *in vitro* and the developed formulations. Hence, this can be viewed as a viable alternative to conservative nasal drops by virtue of its ability to enhance nasal residence time and thereby

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intranasal bioavailability. The ease of administration, coupled with its ability to provide sustained release, could probably result in less frequent administration, thus enhancing patient compliance.

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